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**PROGRAMA DE PÓS-GRADUAÇÃO STRICTU SENSU – MESTRADO EM
ODONTOLOGIA**

ANA CAROLINE LIMA COLOMBINO

**O EFEITO DO TRATAMENTO DE SUPERFÍCIE E DA TERMOCICLAGEM NA
RESISTÊNCIA DE UNIÃO DE UMA CERÂMICA DE ZIRCÔNIA ULTRA-
TRANSLÚCIDA E CIMENTO RESINOSO**

**THE EFFECT OF SURFACE TREATMENT AND THERMOCYCLING ON THE
BOND STRENGTH OF ULTRA-TRANSLUCENT ZIRCONIA CERAMIC AND
RESIN CEMENT**

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Dissertação apresentada ao Programa de Pós-Graduação – Mestrado Acadêmico da Universidade de Uberaba como parte dos requisitos para obtenção do título de Mestre em Odontologia, na área de concentração em Clínica Odontológica Integrada.

Orientador: Prof. Dr. Gilberto Antônio Borges.

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RESUMO

O objetivo desse estudo foi avaliar o efeito do tratamento de superfície e da termociclagem na resistência de união de uma cerâmica de zircônia ultra-translúcida e um cimento resinoso. Cento e vinte amostras de zircônia ultra-translúcida foram confeccionadas para receber um tratamento de superfície específico: Jateamento com óxido de alumínio (OA) e condicionamento de dióxido de zircônia (DZ). Seções de zircônia ($n = 10$) foram distribuídas em 12 grupos de acordo com dois fatores: 1) tratamento e 2) termociclagem, sendo 1) controle (C), silano (S) e primer (P) e 2) sem termociclagem (TC_0), e com termociclagem 10.000 termociclos (TC). Para a aplicação do cimento resinoso, moldes de polivinilsiloxano foram colocados na superfície da cerâmica para determinar a área de união. Removido o excesso de cimento, em seguida foi fotoativado por 20 s, com uma fonte de luz LED. Após a remoção da matriz de silicone as amostras foram testadas em microcisalhamento (μ SBS) 0,5 mm / min após 24h e após a TC. Os dados foram analisados usando o teste de Kruskal-Wallis e teste post hoc de student Newman-Keuls ($\alpha = 0,05$). Para a condição de TC_0 , a média dos grupos (OA + S), (OA + P) e (DZ + S) resultou em maior resistência de união do que os outros grupos (OA + C), (DZ + C) e (DZ + P), sendo $p < 0,005$. Para a condição TC, todos os grupos mostraram uma diminuição significativa na média em comparação com aqueles de 24h. No entanto, os grupos (OA + C) e (DZ + C) não resistiram aos ciclos, não sendo realizado o teste microcisalhamento. Os resultados do presente estudo mostraram a eficácia do jateamento de óxido de alumínio, juntamente com outros agentes de união e com uma resistência de união mais estável após a termociclagem e mais estudos serão necessários para o uso da pasta de dióxido de zircônia e sua concentração ideal.

Palavras chave: Cerâmica, zircônia, tratamento de superfície.

Abstract

The aim of this study was to evaluate the effect of surface treatment and thermocycling on the union strength of an ultra-translucent zirconia ceramic and a resin cement. One hundred and twenty samples of ultra-translucent zirconia were made to receive a specific surface treatment: Aluminum oxide blasting (OA) and zirconia dioxide (DZ) conditioning. Zirconia sections (n = 10) were distributed in 12 groups according to two factors: 1) treatment and 2) thermocycling, where 1) control (C), silane (S) and primer (P) and 2) without thermocycling (TC0), and with thermocycling 10,000 thermocycles (TC). For the application of resin cement, polyvinylsiloxane molds were placed on the ceramic surface to determine the joining area. Removed the excess cement, then was photoactivated for 20 seconds, with an LED light source. After removal of the silicone matrix, the samples were tested in microshear (μ SBS) 0.5 mm / min after 24h and after CT. The data were analyzed using the Kruskal-Wallis test and post hoc student Newman-Keuls test ($\alpha = 0.05$). For the condition of TC0, the media of the groups (OA + S), (OA + P) and (DZ + S) resulted in higher union resistance than the other groups (OA + C), (DZ + C) and (DZ + P), being p 0.005. For the CT condition, all groups showed a significant decrease in media compared to those of 24h. However, the groups (OA + C) and (DZ + C) did not resist the cycles, and the microshear test was not performed. The results of the present study showed the efficiency of aluminum oxide blasting, together with other joining agents and with a more stable union resistance after thermocycling and further studies will be necessary for the use of zirconia dioxide paste and its ideal concentration.

Key words: Ceramics, zirconia, surface treatment.

LISTA DE ABREVIATURAS

OA	Óxido de alumínio
DZ	Dióxido de zircônia
S	Silano
C	Controle
P	Primer
TC	Termociclagem
CAD/CAM	Computer Aid Design and Computer Aid Manufacturing
MPa	MegaPascal
μSBS	Microcisalhamento
h	Horas

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1. Introdução

1 Uma ampla variedade de materiais em odontologia tem sido explorada para
2 substituir dentes perdidos, com o propósito de restaurar função e estética. Entre os
3 materiais dentários, a cerâmica tem se destacado devido sua diversidade de
4 fabricação, e propriedades desejáveis (GALI; K, 2019). Para Venâncio *et al.*, em
5 2013, a cerâmica é o material que reproduz melhor as características ópticas do
6 esmalte e da dentina, como fluorescência, opalescência e translucidez, bem como
7 biocompatibilidade, alta resistência à compressão e à abrasão e estabilidade da cor.

8 O termo cerâmica vem do grego *κέραμος*, que significa matéria-prima
9 queimada, ou seja, para que esse material obtenha propriedades desejáveis, é
10 necessário que ocorra sua queima (BORGES *et al.*,2015). As cerâmicas
11 odontológicas podem se apresentar de diversos tipos, exibindo propriedades
12 químicas, mecânicas, físicas e térmicas que se diferenciam dos outros materiais,
13 além de serem mais resistentes à corrosão e não reagem de imediato com a maioria
14 de líquidos, gases, bases ou ácidos fracos (ANUSAVICE *et al.*, 2013).

15 No fim do século XX, vários sistemas inovadores foram introduzidos para a
16 fabricação de restaurações dentárias de cerâmica pura, que possibilitam um preparo
17 na mesma altura da margem gengival livre, o que leva a um melhor resultado
18 estético sem invadir o espaço biológico (LODI *et al.*, 2017), além de que possui uma
19 melhor adaptação em relação aos materiais metalocerâmicos (BONFANTE *et al.*,
20 2010). De início foi usado um sistema cerâmico-vítreo passível de fundição, no qual
21 a cerâmica era fundida utilizando a técnica de cera perdida e depois recebia
22 tratamento térmico para promover a sua transformação em cerâmica com estrutura
23 vítrea. Com as dificuldades do processamento e alta incidência de fraturas devido a
24 friabilidade do material, esse sistema foi abandonado, permitindo que outros
25 processos fossem mais utilizados para as confecções (POWER; SAGAKUCHI,
26 2012).

27 As cerâmicas podem ser processadas de diferentes maneiras, sendo
28 tradicionalmente aplicadas em camadas ou sobre uma estrutura metálica ou troquel
29 refratário e posteriormente sinterizadas, melhorando a qualidade final do
30 revestimento (SILVA *et al.*,2017). Com a evolução do processamento surgiram os
31 métodos de prensagem isostática e CAD/CAM.

32 Montazerian e Zanotto, em 2016, afirmaram que as cerâmicas podem ser
33 classificadas de acordo com a presença ou ausência de uma fase da matriz de vidro
34 ou de acordo que o material contém uma matriz orgânica altamente preenchida com
35 partículas de cerâmica. Segundo Gracis *et al.*, em 2015, o sistema de classificação
36 das cerâmicas frequentemente usado por Kelly e Benetti, em 2011, pode gerar
37 confusão, uma vez que a cerâmica com predominância de vidro foi proposta de
38 forma que correlaciona a quantidade de vidro e as características estéticas e
39 mecânicas do material. Na fase vítrea, encontra-se propriedades de transmissão de
40 luz, o que possibilita reproduzir as características da translucidez em vários níveis.
41 Já na fase cristalina, o cristal é responsável pela resistência da propagação de
42 trincas devido a formação de uma barreira protetora (MALHEIROS *et al.*, 2013). A
43 fabricação desses materiais foi sendo diferenciada, não apenas com componentes
44 naturais como o feldspato, mas também o uso da cerâmica sintética. Isso resultou
45 em uma melhoria na padronização e controle de qualidade desses materiais.

46 Uma das principais cerâmicas odontológicas é a zircônia que tem evoluído
47 consideravelmente, uma vez que esse material tem resistência mecânica alta com
48 força flexural entre 750 a 1200 Mpa. Tem sido estudada a possibilidade de uso da
49 cerâmica de zircônia em vários tipos de restaurações, inclusive na confecção de
50 facetas devido ao aumento do conteúdo na estabilização por óxido de ítrio
51 (RANGANATHAN *et al.*, 2017). A translucidez das zircônias ultra-translúcidas
52 aumentou suas frações de volume de fase cúbica opticamente isotrópica (> 50%)
53 (YAN *et al.*, 2018), aumentando de 3% mol para 4% mol (4Y-PSZ) ou 5% mol (5Y-
54 PSZ), o que minimiza sua opacidade (LAWSON *et al.*, 2020), tornando-a apropriada
55 para restaurações anteriores monolíticas (MONTEIRO *et al.*, 2020).

56 Todavia, há controvérsia em relação à resistência de união da zircônia, uma
57 vez é inerte, não podendo ser condicionada com ácido fluorídrico (4% - 10%)
58 (JABBAR; DULAMI, 2020). Diante disso, segundo Tholey *et al.*, em 2011, a
59 demanda da cerâmica de zircônia diminuiu para menos de 25%, devido grande
60 preocupação clínica sobre as falhas adesivas, estabilidade a longo prazo, e
61 ocorrência de lascamento. Apesar da falta de informação sobre a maioria dos
62 procedimentos de ligação com eficiência e durabilidade, tem se estudado diversos
63 tratamentos como forma de auxiliar a resistência de união, como deposição de nano-
64 filme de óxidos de silício, a técnica de glaze-on, silanos de aquecimento,

65 condicionamento químico usado para melhor ligação à zircônia (MELO *et al.*, 2015),
66 jateamento com óxido de alumínio, cimento resinoso contendo 10-metacriloxidecil di-
67 hidrogênio monômero de fosfato (10-MDP), primers universais também contendo
68 monômeros de metacrilato, processamento por plasma, infiltração de sílica pelo
69 método sol-gel, infiltração de vidro feldspático, entre outros (SOUZA *et al.*, 2018).

70 Segundo Aung *et al.*, em 2019, o 10-MDP tem apresentado eficácia para
71 promover união à zircônia, um monômero adesivo até então elaborado para se ligar
72 à estrutura dental e ao metal. Tanis e Akcaboy, em 2015, demonstraram que o uso
73 de cimento resinoso contendo 10-MDP tem aumentado significativamente a
74 resistência de união em zircônias que também receberam jateamento com óxido de
75 alumínio.

76 O uso de jateamento de óxido de alumínio é um assunto muito discutido
77 devido suas controversas na literatura (LIMA, 2018). De acordo com Inokoshi *et al.*,
78 em 2014, o jateamento do óxido de alumínio com de partículas de 30 µm na
79 superfície da cerâmica de zircônia com associação de primers/cimentos à base de
80 MDP, pode associar em uma união mais durável à estrutura.

81 Seguindo os estudos de Jo *et al.*, em 2020, o tratamento da superfície da
82 zircônia com a pasta de dióxido de zircônia (ZrO₂) e nanopartículas de carbono,
83 pode aumentar a resistência de união entre a zircônia e a estrutura dental, sendo
84 realizado sobre a superfície da zircônia antes do processo de sinterização. As
85 partículas de ZrO₂ que possui tamanho nanométrico, podem se conectar à superfície
86 da zircônia por ligações de hidrogênio, o que permite que a partícula de carbono
87 produza um material mais poroso após sofrer sinterização.

88 Além do tratamento de superfície da zircônia, outro fator de grande relevância
89 clínica é o envelhecimento por meio das condições térmicas intraorais (ELIASSON;
90 DAHL, 2019). Gale e Darvell, em 1998, já haviam avaliado que as mudanças de
91 temperatura no ambiente bucal poderiam ser alteradas através dos alimentos,
92 bebidas e até mesmo pela respiração, que podem provocar tensões mecânicas e
93 comprometerem a retenção e resistência.

94 Os principais pontos de interesse foram amplamente discutidos, a fim de
95 traçar recomendações clínicas com base em evidências científicas (STAPPERT *et*
96 *al.*, 2005) e, quando ausentes, na prática clínica, juntamente com comunidade
97 científica (ZARONE *et al.*, 2019).

98 Diante disso, objetivo desse trabalho foi avaliar o efeito do tratamento de
99 superfície e da termociclagem na resistência de união de uma cerâmica de zircônia
100 ultra-translúcida. A hipótese nula investigada mostra se ambos materiais possuem
101 resistência iguais ou parecidas para uma resistência de união favorável.

2. Objetivos

102 O objetivo desse estudo foi avaliar o efeito do tratamento de superfície e da
103 termociclagem na resistência de união de uma cerâmica de zircônia ultra-translúcida
104 e cimento resinoso.

105

106 Identificar qual tratamento de superfície será mais eficiente, sendo eles o
107 condicionamento com dióxido de zircônia e jateamento com óxido de alumínio.

108

109 Avaliar o efeito da ciclagem térmica após a cerâmica ser tratada e cimentada,
110 e qual tratamento ofereceu melhor resistência de união por meio do teste de
111 microcisalhamento.

112 **TITLE:** The effect of surface treatment and thermocycling on the bond strength of
113 ultra-translucent zirconia ceramic and resin cement

114

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138 **RUNNING TITLE:** Bond strength of zirconia ceramics before and after thermal
139 fatigue

140 **CLINICAL RELEVANCE:** When zirconia receives a surface treatment, it improves
141 its bond strength to the tooth structure.

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SUMMARY

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153 Objective: To evaluate the bond strength between an ultra-translucent zirconia
154 ceramic and the cementing agent under different surface treatments after 24 hours
155 of water storage (24h) and after 10,000 thermocycles (TC), to evaluate the bonding
156 interface. Materials and methods: One hundred and twenty zirconia samples were
157 prepared and divided into two groups to receive a surface treatment: sandblasting
158 with aluminum oxide (AO) and etching with zirconia dioxide (ZD). Zirconia sections
159 (n = 10) were assigned to 12 groups according to two factors: 1) treatment (control
160 [C], silane [S] and primer [P]) 2) thermocycling (no thermocycling [TC₀], 10,000
161 thermocycles [TC]). For the application of resin cement, polyvinylsiloxane molds
162 were placed on the ceramic surface to determine the adhesion area. Excess cement
163 was removed, then photoactivated for 20 s with a LED light source. After removal of
164 the silicone matrix, the samples were tested in microshear (μ SBS) 1.0 mm/min cross
165 speed after 24h or TC. Data were analyzed using Kruskal-Wallis and Student-
166 Newman-Keuls post hoc test ($\alpha = 0.05$). **Results:** For the TC₀ condition, the mean of
167 the groups (AO + S), (AO + P) and (DZ + S) resulted in higher μ TBS than the other
168 groups (AO + C), (ZD + C) and (ZD + P), where p 0.005. For the TC condition, all
169 groups showed a significant decrease in the mean compared to those at 24h p 005.
170 However, the groups (OA + C + TC) and (DZ + C + TC) did not resist the cycles, and
171 the μ TBS could not be performed. **Conclusions:** The results of the present study
172 showed the effectiveness of aluminum oxide blasting, together with other bonding
173 agents and with a more stable bond strength after thermocycling. However, more
174 studies are needed on zirconia surface treatment.

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177 **Keywords:** Ceramics, zirconia, surface treatment.

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193 1 INTRODUCTION

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195 Dental ceramics have stood out due to their manufacturing diversity and
196 desirable properties so that they can replace lost teeth, restoring function and
197 aesthetics.^{1,2} It is the material that best reproduces optical characteristics of enamel
198 and dentin, such as fluorescence, opalescence and translucency, as well as
199 biocompatibility, high compressive and abrasion strength and color stability.²

200 For this material to obtain desirable properties, it is necessary to burn it,³ and
201 with this, it is possible to present itself in various ways, exhibiting chemical,
202 mechanical, physical and thermal properties that differ from other materials.⁴ Several
203 systems were introduced at the end of the 20th century for the manufacture of pure
204 ceramics, which offer a better adaptation in relation to metaloceramic materials.^{5,6}

205 The ceramic-vitreous system initially used was abandoned due to processing
206 difficulties and high incidence to fractures, which allowed new forms of ceramic
207 making.⁷ Therefore, today ceramics can be processed in different ways, improving the
208 final quality of the coating, especially with the use of CAD/CAM.^{7,8} In addition, they
209 can be classified according to the presence or absence of the glass matrix or
210 according to which the material contains an organic matrix highly filled with ceramic
211 particles, since the classification system can generate confusion, and ceramics with
212 predominance of glass correlate the amount of glass and the aesthetic and mechanical
213 characteristics of the material^{9,10,11,12} The manufacture of these materials was
214 differentiated, not only with natural components such as feldspar, but also the use of
215 synthetic ceramics. This resulted in an improvement in the standardization and quality
216 control of these materials.

217 Zirconia is one of the ceramics that has evolved considerably, since it has high
218 mechanical resistance with flexural strength between 750 to 1200 Mpa. With greater
219 translucency through the increase of the content in the stabilization by yttrium, the
220 possibility of using this ceramic for aesthetic purposes has been researched.¹³ This
221 translucency, especially in ultra-translucent zirconia, increased its volume fraction to
222 optically isotropic cubic phase (> 50%),^{13,14} increasing from 3% mol to 4% mol (4Y-
223 PSZ) or 5% mol (5Y-PSZ), which minimizes its opacity making it suitable for monolithic
224 previous restorations.^{15,16}

225 However, there is controversy regarding the bond strength of zirconia, once it is inert
226 and cannot be conditioned with hydrofluoric acid (4% - 10%)^{17,18} In view of this, there is

227 a decrease in the demand of zirconia ceramics due to great clinical concern about
228 adhesive failures, long-term stability, and occurrence of chipping.¹⁹ Despite the lack of
229 information on most connection procedures with efficiency and durability, several
230 treatments have been studied as a way to aid the bond strength, one of them is
231 aluminum oxide blasting and zirconia dioxide conditioning, the object of this study.^{19,20}
232 The use of aluminum oxide blasting is a subject much discussed due to its
233 controversies in the literature²³.

234 In addition to the surface treatment of zirconia, another factor of great clinical
235 relevance is aging through intraoral thermal conditions.²⁶ Gale and Darvell, in 1998,
236 had already evaluated that temperature changes in the oral environment could be
237 altered through food, beverages and even breathing, which can cause mechanical
238 tensions and compromise retention and resistance.²⁷

239 The main points of interest were widely discussed in order to outline clinical
240 recommendations based on scientific evidence and clinical practice.^{29,30} Therefore,
241 the objective of this work was to evaluate the effect of surface treatment and
242 thermocycling on the union strength of an ultra-translucent zirconia ceramic and a
243 resin cement. The null hypothesis investigated shows whether both materials have
244 equal or similar resistance to a favorable union resistance.

245

246 **2 MATERIALS AND METHODS**

247

248 *2.1 Materials selection*

249 The table 1 shows the materials and their respective manufacturers that were
250 used in the study.

251 *2.2 Surface treatment procedures*

252 A total of 120 samples of high translucent zirconia ceramics (ZirkOM SHT,
253 Odontomega, German) with dimensions 12 mm in width, x 12 mm in depth and 1 mm
254 in thickness were fabricated, following the manufacturer's instructions. After
255 preparation and sintering, the samples were divided into two groups of sixty each,
256 where one group received a surface treatment with blasting of 50µm aluminum oxide
257 (AO) particles (BioArt, São Carlos, Brazil) at a pressure of 5 bar at a distance of 1cm
258 and a sandblasting angle of 45° in relation to the ceramic surface for one minute. The

259 other pre-sintered group will receive, as a surface treatment, application of a zirconia
260 dioxide paste [ZD] (ZirADD, PNUADD, Busan, Korea) at a concentration of 3.0 g per
261 100 g of distilled water. The disks with ZrO₂ paste were taken to the furnace for
262 sintering of the paste in a specific guide (Zirkonzahn, Bolzano, Italy) at a temperature
263 of 1530°C for 12 hours. Then, the two groups were subdivided into three subgroups of
264 twenty samples each. The first subgroup, being the control group (C) received no
265 specific treatment. The second subgroup was the silane (S) (Monobond N, Ivoclar
266 Vivadent, AG Schaan, Liechtenstein) which has a bifunctional molecule that acts as a
267 binding agent. With a fine tip microbrush (KG Sorensen, Cotia, São Paulo, Brazil) it
268 was applied over the ceramic surface, removing the excess with a triple syringe jet for
269 10 seconds, and letting the silanic agent act for 5 minutes. The third group used a
270 ceramic primer (P) with MDP monomer (Clearfil Ceramic Primer, Kuraray, Okayama,
271 Japan). It was passed over the ceramic surface with a microbrush, removing the
272 excess with a triple syringe jet for 10 seconds.

273

274

275 *2.3 Specimens cementation*

276

277 For the application of resin cement (Variolink Esthetic LC, Ivoclar Vivadent AG
278 Schaan, Liechtenstein), polyvinylsiloxane molds (Virtual, Ivoclar Vivadent AG Schaan,
279 Liechtenstein), 0.5 mm thick, with four cylindrical holes (0, 8 mm in diameter) were
280 fabricated and placed on the ceramic surface to determine the bonding area. The
281 resin cement was prepared according to the manufacturer's instructions and inserted
282 into the mold hole with a dentin spoon (Duflex – Juiz de Fora, Minas Gerais, Brazil).
283 Excess cement was removed with a spatula #24 (Duflex, Juiz de Fora, Minas Gerais,
284 Brazil). The holes were filled with resin cement and a polyester transparent strip was
285 placed over the filled holes. A constant and uniform load of 454 gF was applied for 1
286 min using a custom-made device. The resin cement was photoactivated for 20 s in
287 continuous mode with a LED light source (Bluephase, Ivoclar Vivadent AG Schaan,
288 Liechtenstein) with an irradiance of 800 mW / cm², verified with a radiometer (Kerr
289 Sybron, Anaheim, CA, USA). After 10 minutes, the silicone matrix was removed, and
290 the cement cylinders were carefully evaluated under an optical microscope to observe
291 the bonding area. Then, they were stored for 24 hours at 37°C, 100% relative humidity
292 until the bond strength test.

293

294 *2.4 Microshear test (μ SBS) and aging*

295

296 After 24 hours, the groups that underwent thermal cycling (MSCT-3, Marcelo
297 Nucci ME, São Carlos, São Paulo, Brazil) received 10,000 cycles (TC), 10 s in hot
298 water (55°C) and 10 s in cold water (5°C) and then to the microshear test (μ SBS)
299 (figure 1). The test was performed in a test machine (EMIC DL 3000® - EMIC -
300 Equipment and Testing Systems Ltda., São José dos Pinhais, Brazil) with a load cell
301 of 50 kgf. A stainless-steel chisel was attached to the load cell and the test was
302 performed at 0.5 mm/min of cross-velocity until failure occurred. The remaining
303 groups without thermal cycling were submitted only to the microshear test. The
304 average of each resin cement cylinder in the ceramic samples was calculated to
305 obtain the average value of the strength of the title of each block. The test machine
306 software has been configured to provide results in MPa.

307

308 *2.5 Statistical analysis*

309 Statistical analysis was performed using SPSS. Statistical analysis for bond
310 strength was performed using zirconia as an experimental. The average μ TBS
311 obtained from the cylinders of each zirconia sample was used to represent the bond
312 strength. The Shapiro Wilk test was applied to verify normality, where the non-normal
313 distribution can be affirmed for values of $p < 0.05$. The Kruskal-Wallis test was
314 performed to compare the groups available at $p = 0.000$. To compare the average
315 ranks, the post-hoc student-Newman-Keuls was used, with a significance level α of
316 5%.

317

318 **3 RESULTS**

319 For the TC₀ condition, it can be said that the AO + S, AO + P and ZD + S
320 groups obtained greater bond strength with statistically equal values ($p > 0.05$). For the
321 TC condition, all groups showed a significant decrease in the mean compared to those
322 at 24h, with the ZD + S + TC and ZD + P + TC groups having the lowest results
323 ($p < 0.005$). The AO + C, AO + S + TC, AO + P + TC and ZD + S groups did not show
324 statistical differences. The AO + C + TC and ZD + C + TC groups did not resist the
325 thermocycling test, losing all the specimens (Table 2).

326 4 DISCUSSION

327 The present study evaluated the effect of surface treatment and
328 thermocycling on the union strength of ultra-translucent zirconia ceramics and resin
329 cement. After cementing the samples and their respective assays, it was found that
330 the groups that received blasting as treatment resulted in greater union resistance
331 between their certain agents. The present results are in accordance with Le et. al
332 (2019), which showed that aluminum oxide blasting is a micromechanical procedure
333 that aims to increase roughness, allowing greater increase in surface energy and
334 cleaning, and when combined with an adhesive agent result in greater strength.²⁶
335 However, despite increasing the union resistance, blasting can influence the creation
336 of microcracks that, when propagated, can cause cracks and fractures.²⁷ It is
337 noteworthy that the size of the aluminum oxide grain is extremely important, together
338 with the pressure applied at the time of blasting so that it does not become harmful.
339 Particles larger than 100 µm have been shown to result in degradation and reduction
340 of ceramic strength. Al-Harbi et al. (2016), reported that it is possible to strengthen
341 ceramics with the use of self-adhesive cements for penetration of cracks. Therefore,
342 aluminum oxide blasting should be used with caution, always following the
343 manufacturer's recommendations.²⁸

344 Compared to the study by Jo et al, the treatment of the zirconia surface with zirconia
345 paste (ZrO₂) and carbon nanoparticles is recommended its use before the sintering
346 process.²⁹ and these ZrO₂ particles have a nanometric size, which can connect to
347 the surface of zirconia by hydrogen bonds, which allows the carbon particle to
348 produce a more porous material after being sintered. The use of zirconia dioxide
349 paste resulted in low union resistance among the other agents used after treatment,
350 and the same study did not report having performed the aging test for long-term
351 analysis. The paste used in the study at the concentration of 3.0 g per 100 g of
352 distilled water, which was not as effective. It needs further studies on the product
353 and which concentrations would be ideal to achieve a favorable union resistance. In
354 this sense, the present results would not recommend the use of zirconia dioxide
355 paste.

356 Among the surface treatments, we subdivided the groups for the use of a joining
357 agent (silane and ceramic primer). The use of a ceramic primer with 10-MDP
358 associated with aluminum oxide blasting is characterized by high union strength.

359 Primers containing 10-MDP are widely used in dentistry, as they increase the
360 wettability of the structure and create a stability that takes place through its chemical
361 structure formed by an extensive hydrophobic chain carbon spacer, connecting the
362 phosphate group to metal oxides,^{30,31,32} and thus promotes strong connections
363 between dental substrate and material. In addition to its lower water absorption due
364 to its hydrophobic characteristic.^{33,34} The use of Silane Monobond N (Ivoclar
365 Vivadent AG Schaan, Liechtenstein) has brought significant results for both types of
366 zirconia surface treatment, even though some studies report that it is more efficient
367 in ceramics with vitreous structures.³⁵ It has been shown that silane molecules can
368 be activated by the hydrolysis process to effect silanization of the ceramic surface. In
369 this sense as monobond n composition, it is a metallic primer composed of three
370 different functional monomers, namely silane methacrylate, phosphoric
371 methacrylate and sulfide methacrylate, can say that it is capable of providing a chemical
372 connection with the zirconium oxide layer present on the surface of 3Y-TZP
373 (zirconia).³⁶ It can also be said that the pH of the solution used influences the union
374 strength of the zirconia structure, since a process of hydrolysis of the component
375 occurs in the middle of the acid solution.³⁷

376 In this perspective, the results found for ultra-translucency zirconia ceramics
377 do not differ from other zirconia. In fact, zirconia ceramics were considerably altered
378 in terms of aesthetic result, however, the characteristics of the internal surface for
379 cementation were not altered, which the results of the present study confirm. In view
380 of this, the results of this study cannot simply be applied directly to clinical practice,
381 which does not preclude its use. Zirconia ceramics to be used for example with
382 laminated facets need to be cemented adhesively, but the results of the analysis
383 done here with this translucent ceramic made it clear that the clinical application of
384 this type of ceramic for restorations without good retention should not be
385 recommended even with primers that promote better support.

386

387 **5 CONCLUSION**

388

389 The results of the present study showed the efficacy of aluminum oxide blasting,
390 together with other joining agents and with a more stable bond strength after

391 thermocycling. Further studies on the conditioning of zirconia dioxide and its
392 concentration may be more effective for better bond strength are needed.

393

394 **Conflict of interest statement**

395 All authors declare no potential conflicts of interest with respect to the authorship
396 and/or publication of this article.

Materials	Manufacturer	Composition
Zirconia Ceramic	ZirkOM SHT, Odontomega, German	Zirconia, Itrium.
Zirconia oxide slurry	ZirADD PNUADD, Busan, Korea	zirconia and nanoparticles of carbon.
Ceramic Primer	Clearfil Ceramic Primer, Kuraray Okayama, Japan	3-Metacriloxipropiltrim etoxissilano, 10-Metacriloloxidecil di-hidrogephosphate (MDP), etanol.
Silane	Monobond N®, Ivoclar Vivadent, AG Schaan, Liechtenstein	Alcoholic solution of silane methacrylet, phosphoric acid methacryletand sulfide methacrylet.
Aluminum oxide particle	BioArt® São Carlos, Brasil	Aluminum oxide
Polivilsiloxane	Virtual, Ivoclar Vivadent, AG Schaan, Liechtenstein	Polivinsiloxane, silicone dioxide, aluminum inorganic filler (CAS 1318-02-1), metil hidrogen siloxane.
Resin cement	Variolink Esthetic LC®, IvoclarVivadent, AG Schaan, Liechtenstein	Uretane Dimethacrylate and other methacrylayte monomers, trifluorete of iterbium and mixed espheroid oxides, initiators, stabilizers, and pigments.

Table 1. Materials used in the study.

Condition	Surface treatment					
	Aluminum oxide			Zirconia dioxide		
	Control	Silane	Primer	Control	Silane	Primer
24 hours	2,27(0,67-4,33) ^C	6,61(3,78-16,4) ^A	7,82(1,75-23,3) ^A	1,12(0,17-3,42) ^C	6,21(1,82-21,5) ^{AB}	4,16(0,52 9,46) ^B
Thermocycling	x	2,55(1,19-4,09) ^C	2,01(0,41-5,06) ^C	x	0,46(0,24-0,96) ^D	,58(0,22-1,74) ^D

Table 2. Median, maximum and minimum of the tested groups. Capital letters equal, denote there is no significant difference between comparisons ($p > 0.05$).

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532

533

Conclusão

534 Portanto, de acordo com a metodologia empregada, e com as limitações do
535 presente estudo, concluímos que o tratamento com óxido de alumínio resultou em
536 uma maior resistência de união associado a outros agentes e melhores resultados
537 aos testes de envelhecimento. Serão necessários mais estudos sobre o
538 condicionamento com dióxido de zircônia e sua concentração ideal para a avaliação
539 de resistência de união sobre a estrutura da zircônia.

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Apêndice A – Cimentação das amostras

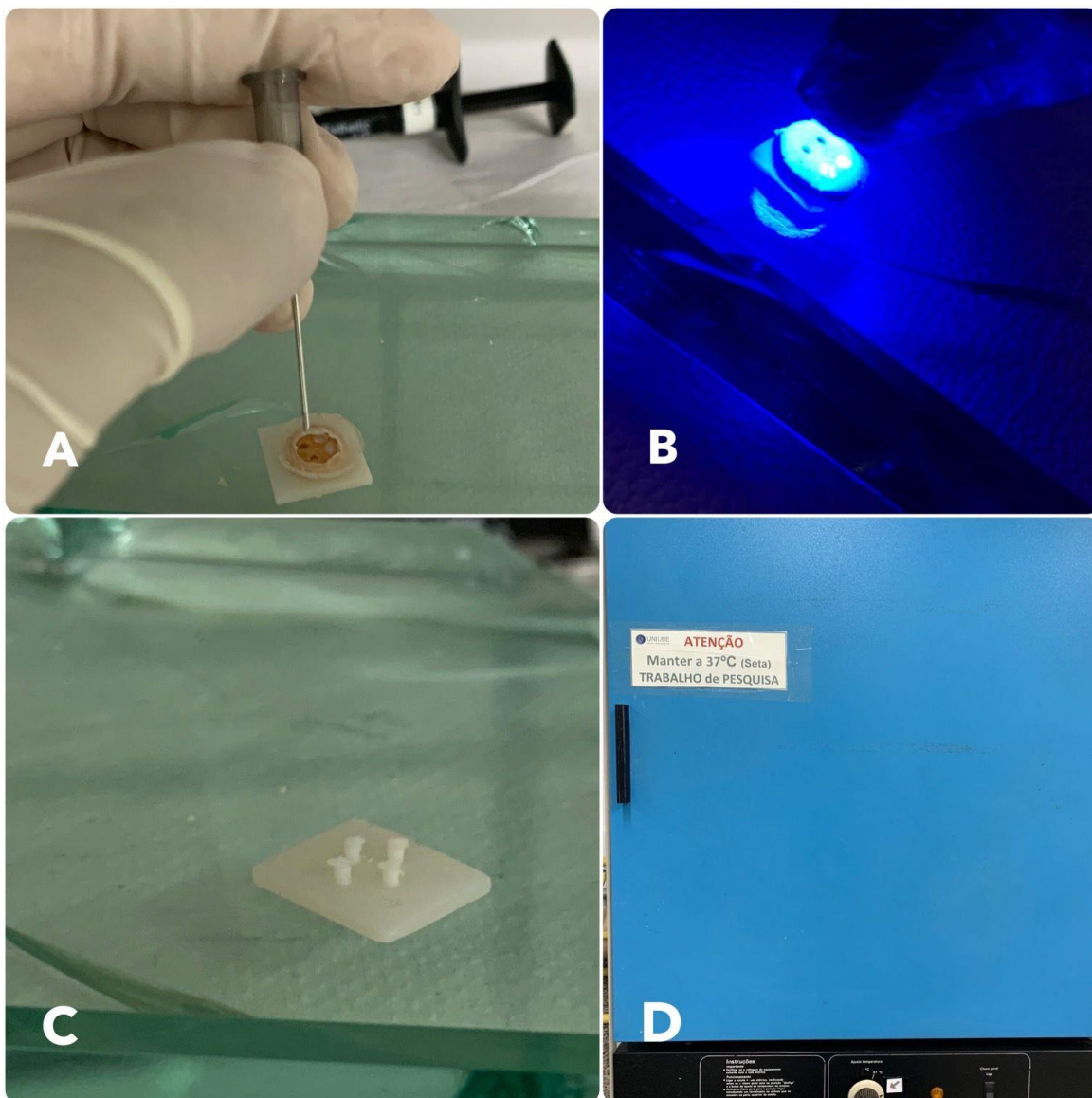


Imagem 1. Cimentação das amostras. A – Amostra da zircônia no momento da cimentação. B – Fotoativação do cimento resinoso. C – Corpos de prova após cimentação na superfície da zircônia. D – Armazenamento das amostras na estufa em temperatura de 37°.

APÊNDICE B – Teste de microcisalhamento

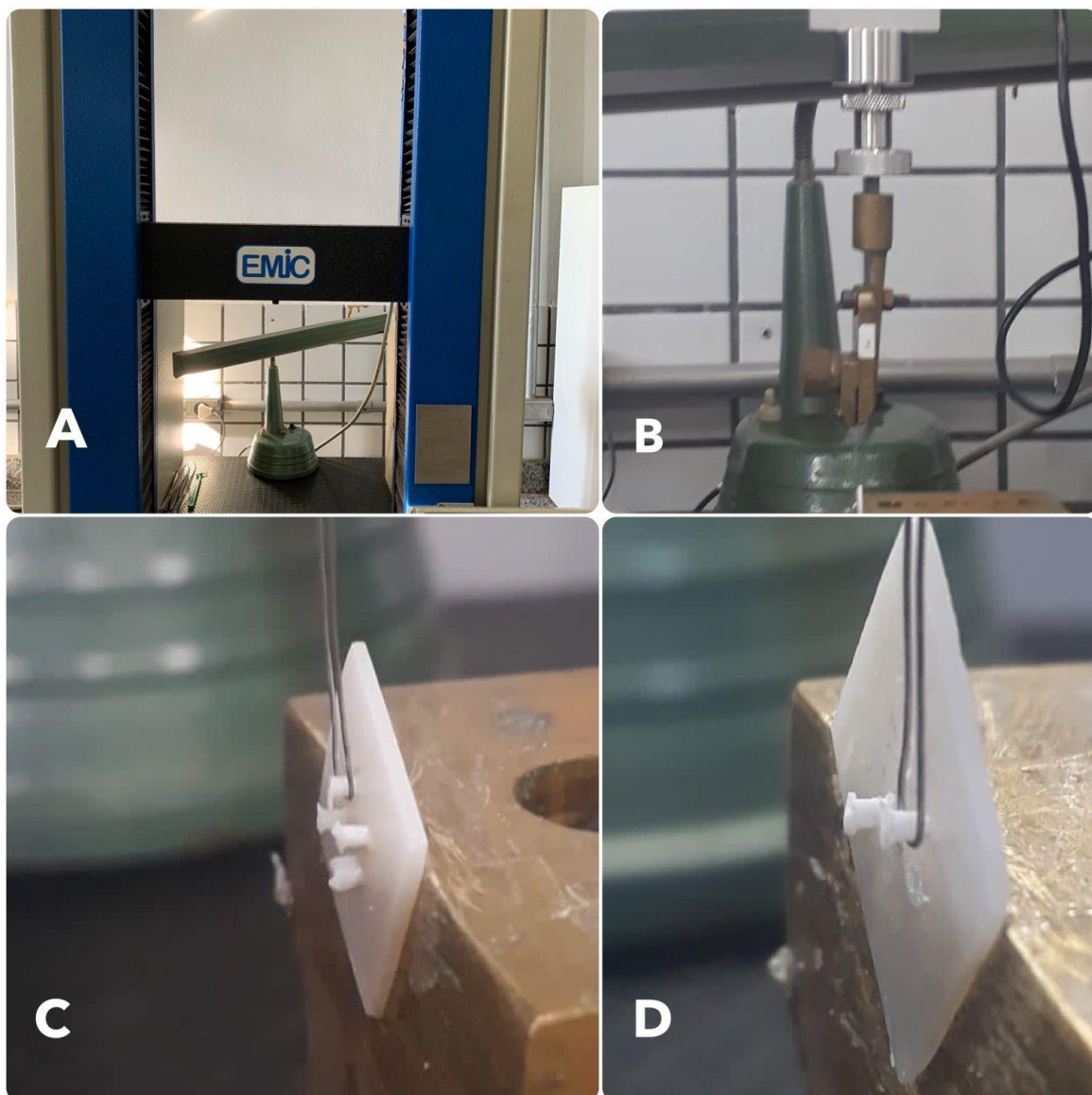


Imagem 2. Teste de microcisalhamento. A – Máquina de teste. B – Cinzel de carga onde a amostra da cerâmica de zircônia foi presa a célula. C – Célula de carga presa ao corpo de prova até que ocorra falha. D – Amostra de zircônia após a falha.

APÊNDICE C – Análise após os testes

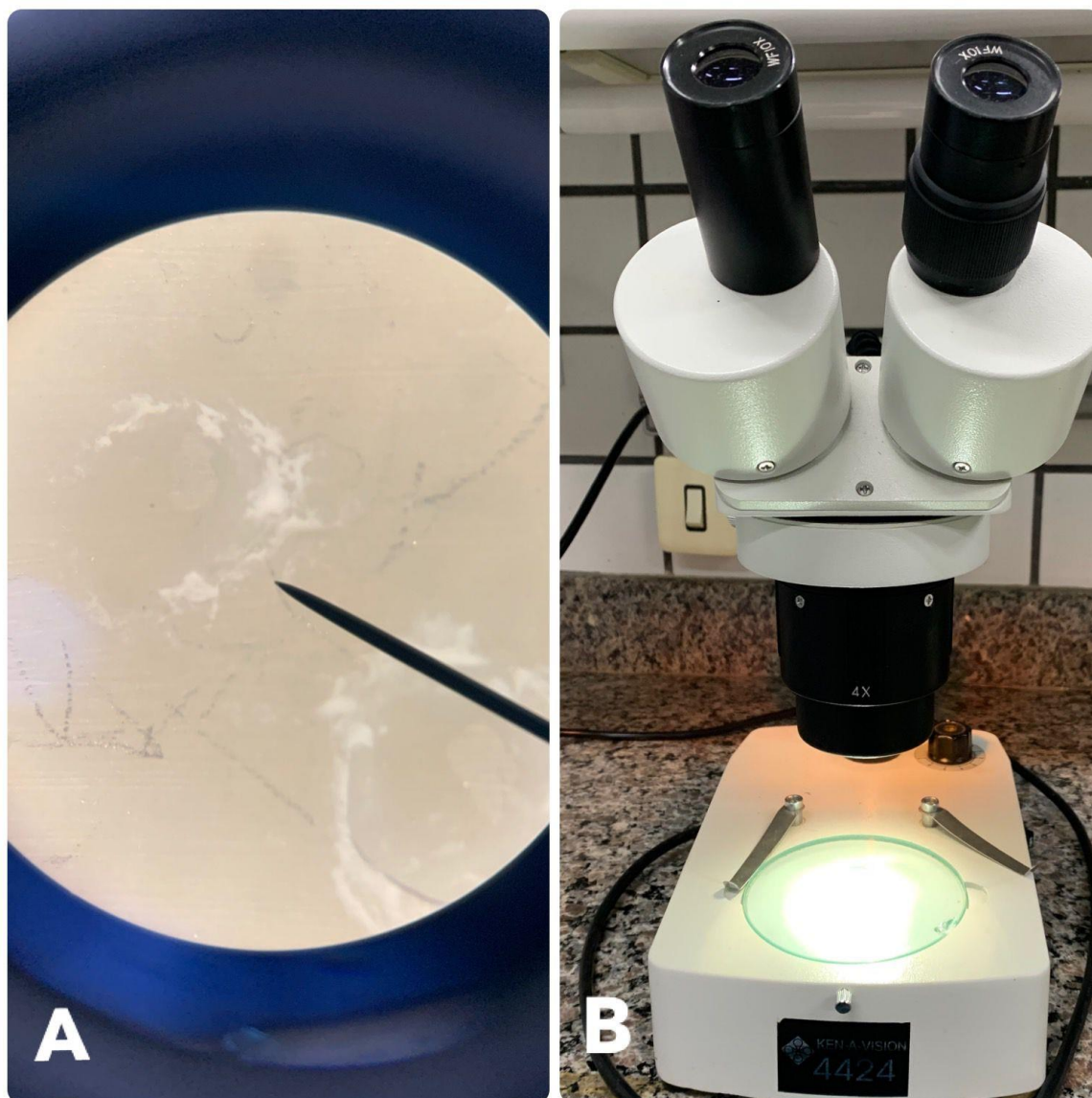


Imagem 3. Análise após os testes. A – Imagem de 400x da amostra de zircônia após os testes. B – Lupa de aumento.

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